

# Data Augmentation in High Dimensional Low Sample Size Setting with Geometry-Aware Variational Autoencoders

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  - The framework
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  - Materials
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# Main Challenges

## Main challenges with medical data

- Small data sets:
  - potential poor subject variability
  - no statistically significant results
  - overfitting
- Large data (e.g. fMRI)  $\implies$  thousands of dimensions

## Need for

- Data augmentation
- Dimensionality reduction

## A solution ?

- Variational Autoencoders

## Issue

- Unable to generate faithfully with small data sets

# Classic Data Augmentation

- Adding some geometric transformations (shift, rotations ...)
- Adding noise, blur ...

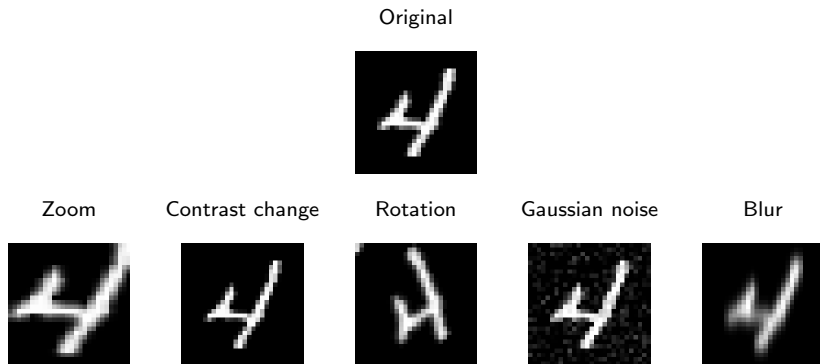


Figure: Examples of transformations

# Classic Data Augmentation - Shortcomings

## Classic DA

- Is data set dependent
- May require the intervention of an expert “knowledge”

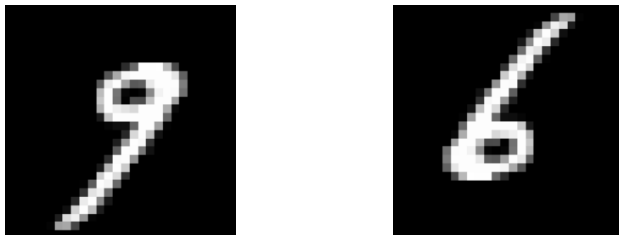


Figure: Nine figure rotated.

## An attractive solution ?

- Generative models (Generative Adversarial Networks, Variational Auto-Encoders ...)

# Use of Generative Models for DA

GANs have already seen a wide use in many fields of application including medicine [YWB19]:

- Magnetic Resonance Images (MRI) [STR<sup>+</sup>18, CMST17]
- Computed Tomography (CT) [FADK<sup>+</sup>18, SYPS19]
- X-ray [MMKSM18, SVD<sup>+</sup>18, WGG<sup>+</sup>20],
- Positron Emission Tomography (PET) [BKK<sup>+</sup>17],
- Mass spectroscopy data [LZL<sup>+</sup>19],
- Dermoscopy [BAN18]
- Mammography [KRO<sup>+</sup>18, WWCL18]

⇒ Most of these studies involved either a quite large training set (above 1000 training samples) or quite small dimensional data.

⇒ As of today, the HDLSS setting remains poorly explored.

⇒ Use VAEs!

# VAE - The Idea

- An auto-encoder based model...

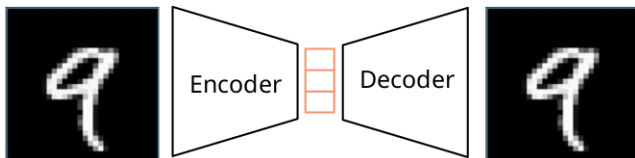


Figure: Simple Auto-Encoder

- ... but where an input data point is encoded as a **distribution** defined over the latent space [KW14, RMW14]

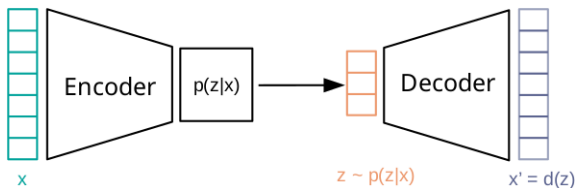


Figure: VAE framework

# VAE - Mathematical Considerations

- Let  $x \in \mathcal{X}$  be a set of data and  $\{P_\theta, \theta \in \Theta\}$  a parametric model
- We assume there exists latent variables  $z \in \mathcal{Z}$  living in a smaller space such that the marginal likelihood writes

$$p_\theta(x) = \int p_\theta(x|z)q_{\text{prior}}(z)dz,$$

where  $q_{\text{prior}}$  is a prior distribution over the latent variables and  $p_\theta(x|z)$  is referred to as the decoder

$$q_{\text{prior}} = \mathcal{N}(0, I), \quad p_\theta(x|z) = \prod_{i=1}^D \mathcal{B}(\pi_{\theta_i}(z))$$

Objective:

- Maximizing the likelihood of the model

Problem:

- The integral is often intractable making  $p_\theta(z|x) = \frac{p_\theta(x|z)q_{\text{prior}}(z)}{p_\theta(x)}$  intractable  
 $\implies$  Bayesian Inference is unusable



# The ELBO

- We have to use Variational Inference

$$q_{\phi}(z|x) \simeq p_{\theta}(z|x),$$

where  $q_{\phi}(z|x) = \mathcal{N}(\mu_{\phi}(x), \Sigma_{\phi}(x))$

- This leads to an unbiased estimate of the log-likelihood

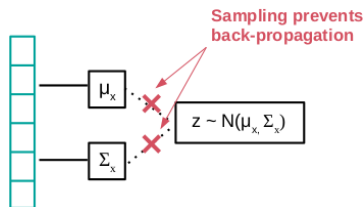
$$\hat{p}_{\theta}(x) = \frac{p_{\theta}(x, z)}{q_{\phi}(z|x)}, \quad \mathbb{E}_{z \sim q_{\phi}(z|x)}[\hat{p}_{\theta}(x)] = p_{\theta}(x),$$

- Taking the logarithm of the expectation we have

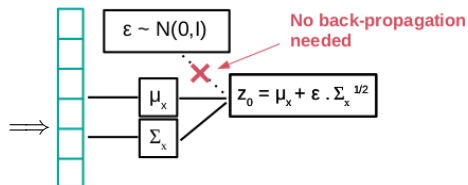
$$\begin{aligned} \log p_{\theta}(x) &= \log \mathbb{E}_{z \sim q_{\phi}(z|x)}[\hat{p}_{\theta}(x)] \\ &\geq \mathbb{E}_{z \sim q_{\phi}(z|x)}[\log(\hat{p}_{\theta}(x))] \\ &\geq \mathbb{E}_{z \sim q_{\phi}(z|x)}[\log(p_{\theta}(x, z)) - \log(q_{\phi}(z|x))] \\ &\geq \text{ELBO} \end{aligned}$$

# The Reparametrization Trick

- Since  $z \sim \mathcal{N}(\mu_\phi(x), \Sigma_\phi(x))$ , the model is not amenable to gradient descent



(a) Back-propagation impossible



(b) Back-propagation possible

$\Rightarrow$  Optimization with respect to encoder and decoder parameters made possible !

# Generating new samples

- We only need to sample  $z \sim \mathcal{N}(0, I)$  and feed it to the decoder.

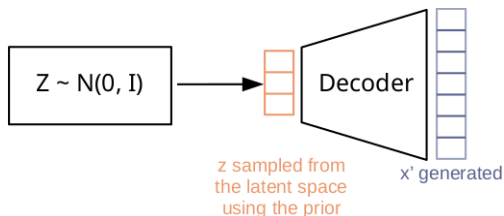


Figure: Generation procedure

Pros:

- Very simple to use in practice

Cons:

- The prior and posterior are not expressive enough to capture complex distributions
- Poor latent space prospecting

# Defining a New Framework

## Assumptions:

- As of now the latent space structure was supposed to be Euclidean (i.e.  $\mathcal{Z} = \mathbb{R}^d$ )
- Let us now relax this hypothesis and assume that  $\mathcal{Z}$  is a Riemannian manifold endowed with a metric  $\mathbf{G}$ .
- It was shown that exploiting the geometrical aspect of probability distributions can lead to far more efficient sampling [GCC09, GC11]

## Our ideas:

- 1 Exploit the manifold structure of the latent space to improve the posterior sampling [CMA20]
- 2 Learn the metric defined in the latent space [CMA20]
- 3 Use the learned geometry to generate instead of the prior [CTSBA21]

# 1) Improve Posterior Sampling - Riemannian HMC

- The idea relies on the **Riemannian** Hamiltonian Monte Carlo Sampler [GC11]
- Simulates the evolution  $(z(t), v(t))$  of a particle whose motion is governed by Hamiltonian dynamics and having a potential  $U(z)$  and kinetic energy  $K(v, z)$

$$U(z) = -\log p_{\text{target}}(z), \quad K(v, z) = \frac{1}{2} v^{\top} \mathbf{G}^{-1}(z) v.$$

- Use of the “Generalized” Leapfrog integrator to sample from  $p_{\text{target}}$
- The target density  $p_{\text{target}}$  is proportional to the true posterior:

$$p_{\theta}(z|x) = \frac{p_{\theta}(x, z)}{p_{\theta}(x)} \propto p_{\theta}(x, z) = p(x|z)p(z) = p_{\text{target}}(z).$$

Pros:

- Posterior sampling is guided by the gradient of the true posterior
- Use the underlying geometry of the data to improve sampling

Cons:

- The metric is unknown

## 2) Learn the Metric - The Choice of the Metric

- We propose to parametrize the metric as follows [Lou19]:

$$\mathbf{G}^{-1}(z) = \sum_{i=1}^N L_{\psi_i} L_{\psi_i}^{\top} \exp\left(-\frac{\|z - c_i\|_2^2}{T^2}\right) + \lambda I_d,$$

- $L_{\psi_i}$  are lower triangular matrices parametrized using neural networks
- $T$  is a temperature to smooth the metric
- $c_i$  are the centroids
- $\lambda$  is a regularization factor

Pros:

- Closed-form expression of the inverse metric  $\implies$  useful for geodesic computation
- Metric volume element  $\sqrt{\det \mathbf{G}(z)}$  easily scalable through  $\lambda \implies$  geodesics travel through most populated areas

# The Model - Riemannian Hamiltonian VAE

- The graphical scheme

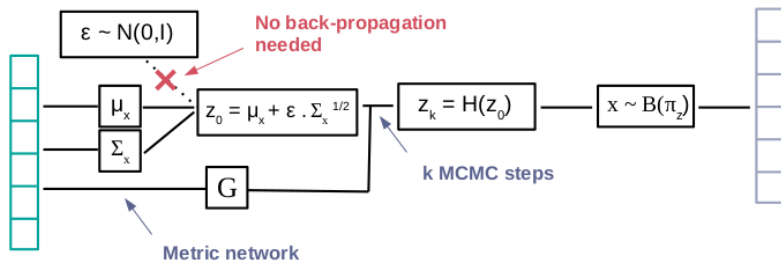
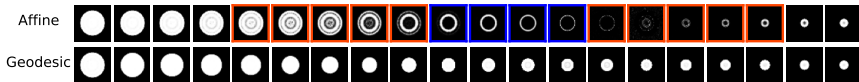
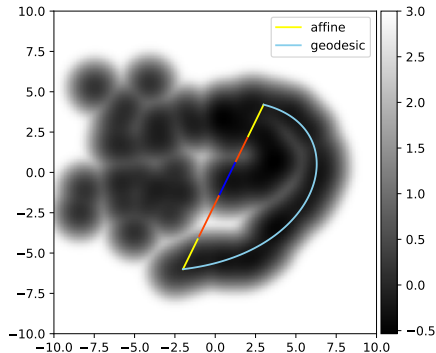
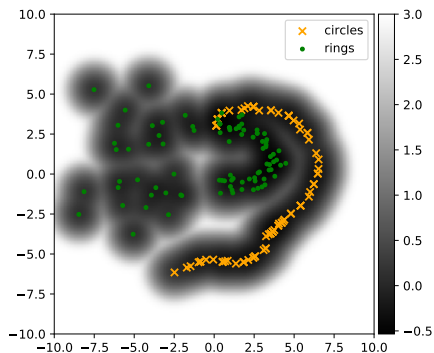


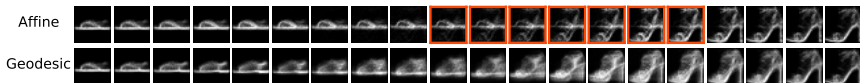
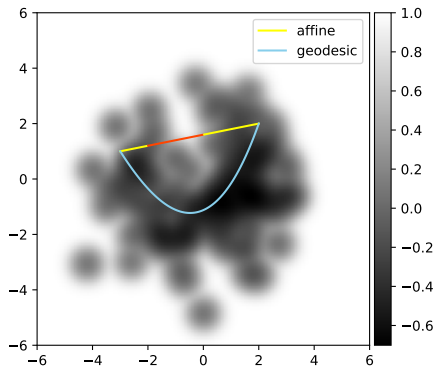
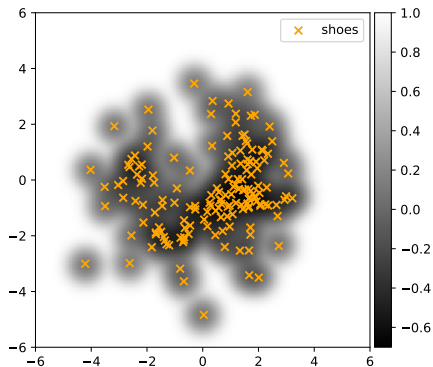
Figure: Riemannian Hamiltonian VAE.

# The Learned Latent Space





# The Learned Latent Space



### 3) Improve Data Generation - Sample With the Metric

Idea:

- Our idea is to use a geometry-based sampling procedure

$$p(z) = \frac{\rho_S(z) \sqrt{\det \mathbf{G}^{-1}(z)}}{\int_{\mathbb{R}^d} \rho_S(z) \sqrt{\det \mathbf{G}^{-1}(z)} dz},$$

where  $S$  is a compact set and  $\rho_S(z) = 1$  if  $z \in S$ , 0 otherwise.

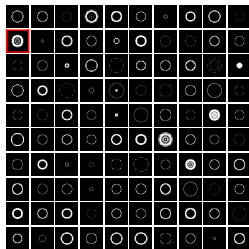
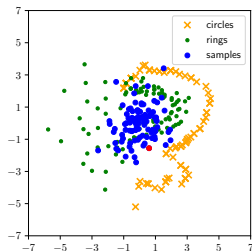
- Use of classic MCMC sampler (e.g. Hamiltonian Monte Carlo)

Pros:

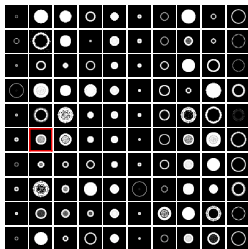
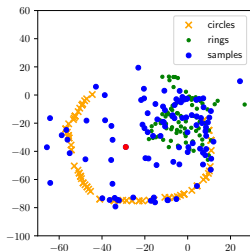
- $\mathbf{G}^{-1}$  easily computable
- Samples “close” to the data

# Sampling Comparison

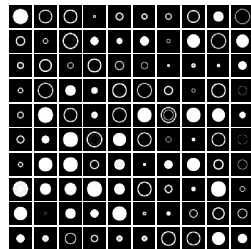
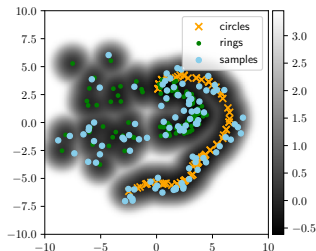
(a) VAE -  $\mathcal{N}(0, I)$



(b) VAE - VAMP (multimodal)



(c) Ours



# Sampling Comparison - Higher Dimension

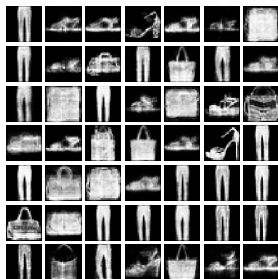
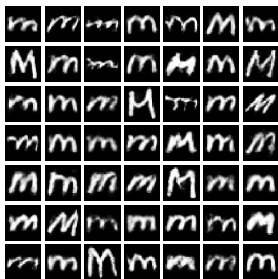
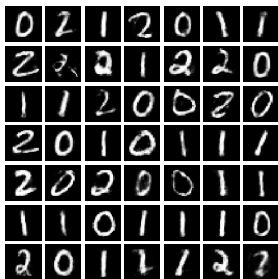
(a) *reduced* MNIST (120)



(b) *reduced* EMNIST (120)



(c) *reduced* Fashion (120)



## Data Augmentation

# Data Augmentation - Framework

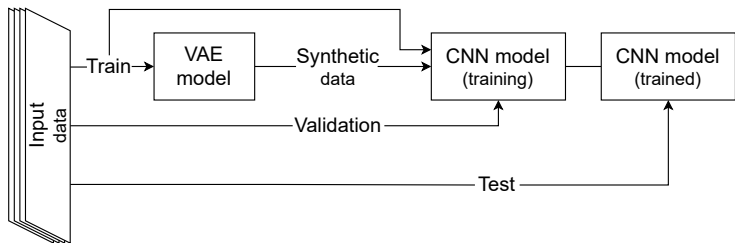


Figure: Data Augmentation framework

1. Toy Data
2. Medical Imaging

# Robustness Across Data Sets

Table: Classification results on *reduced* data sets ( $\sim 50$  samples per class)

	MNIST	MNIST (unbal.)	EMNIST (unbal.)	FASHION
Baseline	$89.9 \pm 0.6$	$81.5 \pm 0.7$	$82.6 \pm 1.4$	$76.0 \pm 1.5$
Baseline + Synthetic				
Basic Augmentation (X5)	$92.8 \pm 0.4$	$86.5 \pm 0.9$	$85.6 \pm 1.3$	$77.5 \pm 2.0$
Basic Augmentation (X10)	$88.2 \pm 2.2$	$82.0 \pm 2.4$	$85.7 \pm 0.3$	$79.2 \pm 0.6$
Basic Augmentation (X15)	$92.8 \pm 0.7$	$85.8 \pm 3.4$	$86.6 \pm 0.8$	$80.0 \pm 0.5$
VAE - 200*	$88.5 \pm 0.9$	$84.0 \pm 2.0$	$81.7 \pm 3.0$	$78.6 \pm 0.4$
VAE - 2k*	$92.2 \pm 1.6$	$88.0 \pm 2.2$	$86.0 \pm 0.2$	$79.3 \pm 1.1$
Ours-200	$91.0 \pm 1.0$	$84.1 \pm 2.0$	$85.1 \pm 1.1$	$77.0 \pm 0.8$
Ours-500	$92.3 \pm 1.1$	$87.7 \pm 0.9$	$85.1 \pm 1.1$	$78.5 \pm 0.9$
Ours-1k	$93.2 \pm 0.8$	<b><math>89.7 \pm 0.8</math></b>	$87.0 \pm 1.0$	<b><math>80.2 \pm 0.8</math></b>
Ours-2k	<b><math>94.3 \pm 0.8</math></b>	$89.1 \pm 1.9$	<b><math>87.6 \pm 0.8</math></b>	$78.1 \pm 1.8$

\* Using a standard normal prior to generate

- Classic DA is data set dependent
- Vanilla VAE performs as well as classic DA



# Robustness Across Data Sets

**Table:** Classification results on *reduced* data sets ( $\sim 50$  samples per class) on synthetic samples only

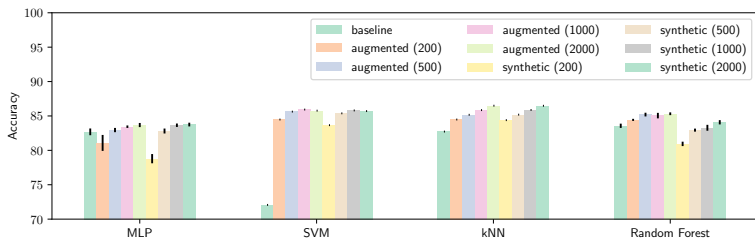
	MNIST	MNIST (unbal.)	EMNIST (unbal.)	FASHION
Baseline	$89.9 \pm 0.6$	$81.5 \pm 0.7$	$82.6 \pm 1.4$	$76.0 \pm 1.5$
Synthetic Only				
VAE - 200*	$69.9 \pm 1.5$	$64.6 \pm 1.8$	$65.7 \pm 2.6$	$73.9 \pm 3.0$
VAE - 2k*	$86.5 \pm 2.2$	$79.6 \pm 3.8$	$78.8 \pm 3.0$	$76.7 \pm 1.6$
Ours-200	$87.2 \pm 1.1$	$79.5 \pm 1.6$	$77.0 \pm 1.6$	$77.0 \pm 0.8$
Ours-500	$89.1 \pm 1.3$	$80.4 \pm 2.1$	$80.2 \pm 2.0$	$78.5 \pm 0.8$
Ours-1k	$90.1 \pm 1.4$	$86.2 \pm 1.8$	$82.6 \pm 1.3$	$79.3 \pm 0.6$
Ours-2k	$92.6 \pm 1.1$	$87.5 \pm 1.3$	$86.0 \pm 1.0$	$78.3 \pm 0.9$

\* Using a standard normal prior to generate

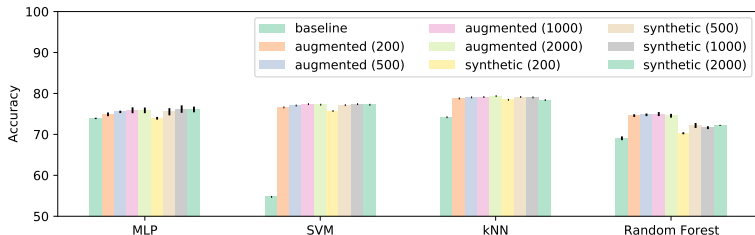
- The proposed model seems to create diverse samples relevant to the classifier

# Robustness Across Classifiers

(a) *reduced* MNIST balanced



(b) *reduced* MNIST unbalanced



# A Note on the Method Scalability

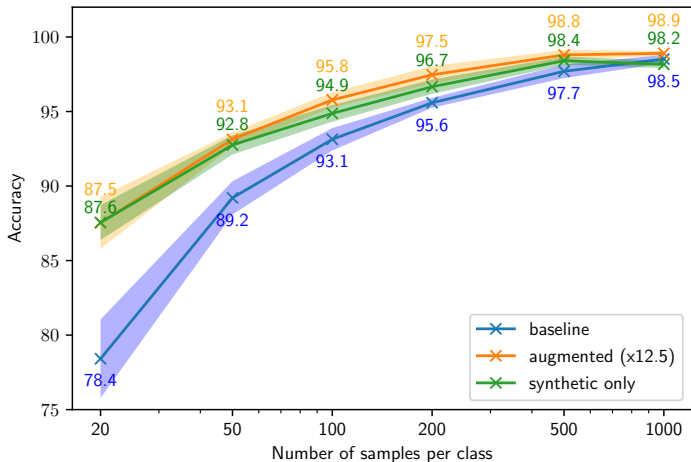


Figure: Benchmark classifier accuracy according to the number of samples in the training set on MNIST.

1. Toy Data
2. Medical Imaging

Classification task: Alzheimer's disease patients (**AD**) vs Cognitively Normal participants (**CN**) using T1-weighted MR images.



**Table:** Summary of participant demographics, mini-mental state examination (MMSE) and global clinical dementia rating (CDR) scores at baseline.

Data set	Label	Obs.	Age	Sex M/F	MMSE	CDR
ADNI	CN	403	73.3 $\pm$ 6.0	185/218	29.1 $\pm$ 1.1	0: 403
	AD	362	74.9 $\pm$ 7.9	202/160	23.1 $\pm$ 2.1	0.5: 169, 1: 192, 2: 1
AIBL	CN	429	73.0 $\pm$ 6.2	183/246	28.8 $\pm$ 1.2	0: 406, 0.5: 22, 1: 1
	AD	76	74.4 $\pm$ 8.0	33/43	20.6 $\pm$ 5.5	0.5: 31, 1: 36, 2: 7, 3: 2

# MRI preprocessing

Bias field correction (N4ITK) + linear registration (ANTs) + cropping

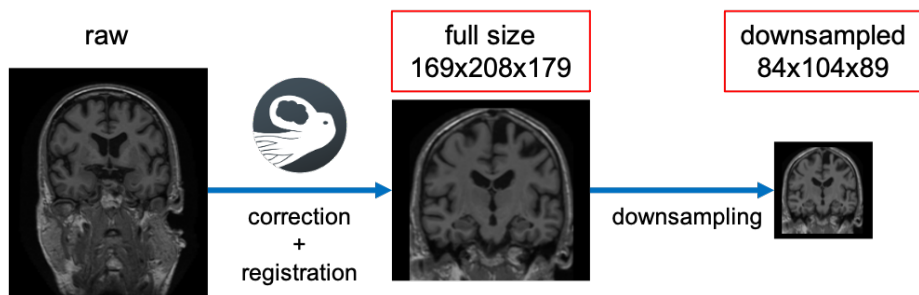
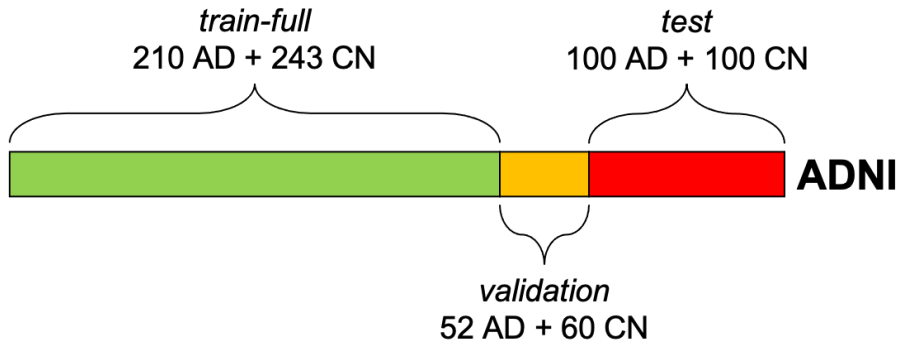


Figure: Preprocessed MRI used in the study

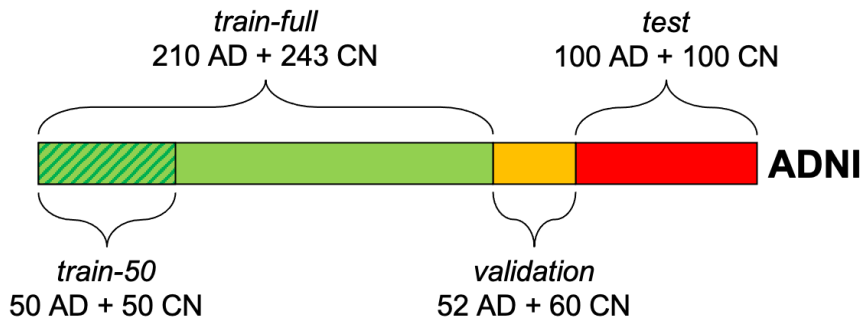
Find wonderful data at:

`/network/lustre/dtlake01/aramis/datasets/adni/caps/caps_v2021`

# Evaluation procedure

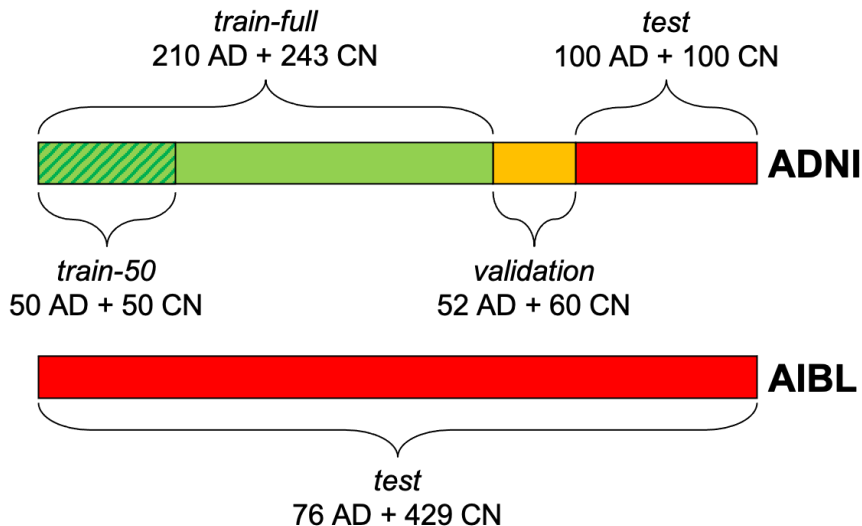


# Evaluation procedure





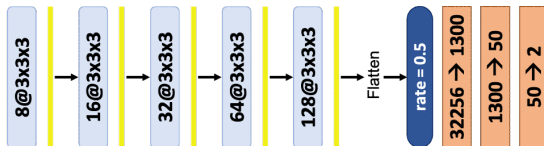
# Evaluation procedure



# CNN architectures

Baseline architectures provided by a previous study [WTSDM<sup>+</sup>20]

## 1. Full size image



## 2. Downsampled image



3D Convolution (stride=1, padding=1) + Batch normalization + LeakyReLU

MaxPooling (kernel=2, stride=2)

Dropout

Fully-connected layer (+ LeakyReLU except last layer)

# CNN architectures

Optimized architectures found with random search procedure (ClinicaDL)

## 1. Full size image



## 2. Downsampled image



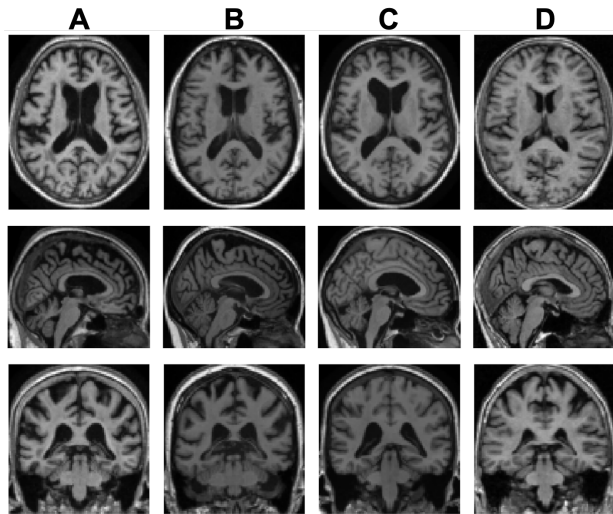
- 3D Convolution (stride=1, padding=1) + Batch normalization + LeakyReLU
- MaxPooling (kernel=2, stride=2)
- Dropout
- Fully-connected layer (+ LeakyReLU except last layer)

Four series of experiments:

- **baseline** architecture on *train-50*
- **baseline** architecture on *train-full*
- **optimized** architecture on *train-50*
- **optimized** architecture on *train-full*

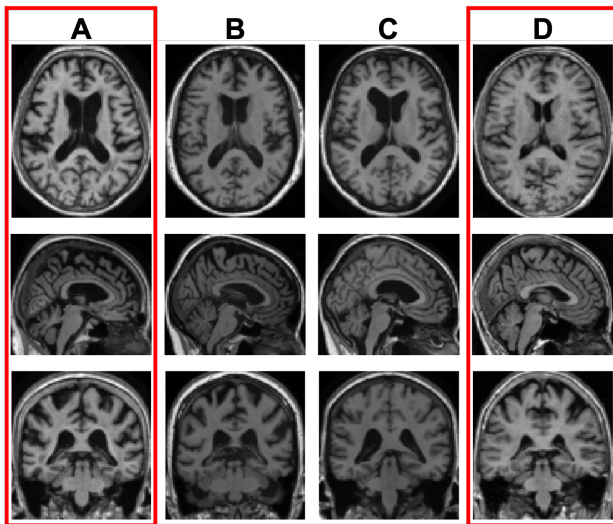
For each experiment 20 CNNs are run and the performance is the mean value of the 20 performance values.

# Synthesized images



**Figure:** Example of two *true* patients compared to two generated by our method. Can you find the intruders ?

# Synthesized images



**Figure:** Example of two *true* patients compared to two generated by our method. Can you find the intruders ?

# Results on train-50 with baseline CNN

**Table:** Mean test performance of each series of 20 runs trained with the **baseline** hyperparameters on *train-50* set.

data set	ADNI balanced accuracy	AIBL balanced accuracy
real	66.3 ± 2.4	67.2 ± 4.1
real (high-resolution)	67.9 ± 2.3	66.5 ± 3.0
500 synthetic + real	69.4 ± 1.6	68.5 ± 2.5
1000 synthetic + real	70.5 ± 2.1	70.6 ± 3.1
2000 synthetic + real	71.2 ± 1.6	72.8 ± 2.2
3000 synthetic + real	72.6 ± 1.6	73.6 ± 3.0
5000 synthetic + real	<b>74.1 ± 2.2</b>	<b>76.1 ± 3.6</b>
10000 synthetic + real	74.0 ± 2.7	74.9 ± 3.2

Increase of balanced accuracy of 6.2 points on ADNI and 8.9 points on AIBL

# Results on train-full with baseline CNN

**Table:** Mean test performance of each series of 20 runs trained with the **baseline** hyperparameters on *train-full* set.

data set	ADNI balanced accuracy	AIBL balanced accuracy
real	77.7 ± 2.5	78.4 ± 2.4
real (high-resolution)	80.6 ± 1.1	80.4 ± 2.6
500 synthetic + real	82.2 ± 2.4	82.9 ± 2.5
1000 synthetic + real	84.4 ± 1.8	83.7 ± 2.3
2000 synthetic + real	85.9 ± 1.6	83.8 ± 2.2
3000 synthetic + real	85.8 ± 1.7	84.4 ± 1.8
5000 synthetic + real	85.7 ± 2.1	84.2 ± 2.2
10000 synthetic + real	<b>86.3 ± 1.8</b>	<b>85.1 ± 1.9</b>

Increase of balanced accuracy of 5.7 points on ADNI and 4.7 on AIBL



# Results on train-50 with optimized CNN

**Table:** Mean test performance of each series of 20 runs trained with the **optimized** hyperparameters on *train-50* set.

data set	ADNI balanced accuracy	AIBL balanced accuracy
real	75.5 ± 2.7	75.6 ± 4.1
real (high-resolution)	72.1 ± 3.1	71.2 ± 5.1
500 synthetic + real	75.6 ± 2.5	76.0 ± 4.2
1000 synthetic + real	77.8 ± 2.3	80.9 ± 3.2
2000 synthetic + real	76.9 ± 2.4	80.0 ± 3.6
3000 synthetic + real	77.8 ± 1.9	81.2 ± 3.7
5000 synthetic + real	76.9 ± 2.5	80.9 ± 2.7
10000 synthetic + real	<b>78.0 ± 2.1</b>	<b>81.9 ± 2.2</b>

Increase of balanced accuracy of 2.5 points on ADNI and 6.3 points on AIBL

# Results on train-full with optimized CNN

**Table:** Mean test performance of each series of 20 runs trained with the **optimized** hyperparameters on *train-full* set.

data set	ADNI balanced accuracy	AIBL balanced accuracy
real	85.5 ± 2.4	81.9 ± 3.2
real (high-resolution)	85.7 ± 2.5	84.4 ± 1.7
500 synthetic + real	86.0 ± 1.8	83.2 ± 2.4
1000 synthetic + real	86.5 ± 1.9	83.7 ± 2.0
2000 synthetic + real	<b>87.2 ± 1.7</b>	84.0 ± 2.0
3000 synthetic + real	85.8 ± 2.6	83.6 ± 3.2
5000 synthetic + real	86.4 ± 1.3	83.5 ± 2.2
10000 synthetic + real	86.7 ± 1.8	<b>84.3 ± 1.8</b>

Increase of balanced accuracy of 1.5 point on ADNI and -0.1 point on AIBL

# Conclusion

Validation of a new VAE-based data augmentation framework on classification tasks on *toy* and *real-life* data sets.

Strengths:

- **Data set generalization** from 2D images (MNIST, EMNIST, FASHION) to 3D medical images (ADNI and AIBL),
- **Classifier independence** MLP, random forest, k-NN and SVM (on toy data sets) ; baseline and optimized parameters (on medical images).
- **Synthetic data relevance** classifiers achieved a similar or better classification performance when trained only on synthetic data than on the *real* train set.
- **Low sample size data sets usability** adding synthetic data improves classification performance even with a small training set (*train-50*)

Validation of a new VAE-based data augmentation framework on classification tasks on *toy* and *real-life* data sets.

Limitations - what could be improved:

- no extensive search on VAE hyperparameters.
- can it be easily coupled with other techniques to limit overfitting?
- would it benefit from the use of longitudinal data?
- *train-50* is still large compared to some medical data sets. . .

Thank you !

## Appendices

# Clustering

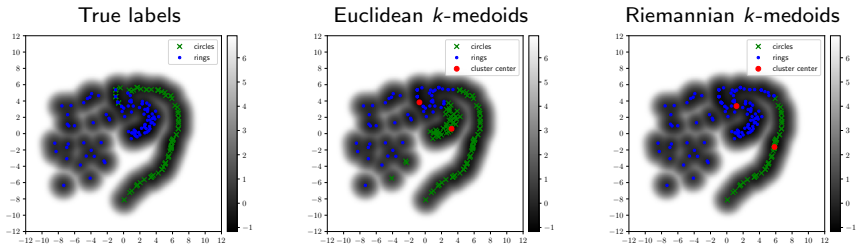


Figure: Euclidean and Riemannian  $k$ -medoids clustering.

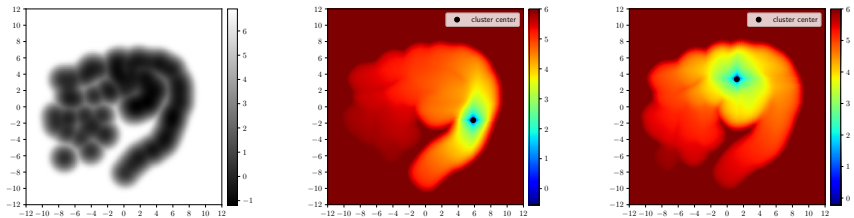


Figure: Distance maps.

# Results - Clustering

Data set	Model	Subset 1	Subset 2	Subset 3	Mean
Synthetic data	linear	53.88	62.52	71.63	62.68
	geodesic	<b>71.41</b>	<b>81.39</b>	<b>79.49</b>	<b>77.43</b>
MNIST 1	linear	89.73	93.11	91.80	91.55
	geodesic	<b>91.68</b>	<b>94.51</b>	<b>95.63</b>	<b>93.94</b>
MNIST 2	linear	68.24	69.22	79.05	71.17
	geodesic	<b>70.35</b>	<b>71.34</b>	<b>79.64</b>	<b>73.78</b>
MNIST 3	linear	75.55	75.76	81.70	77.67
	geodesic	<b>76.08</b>	<b>77.94</b>	<b>81.96</b>	<b>78.66</b>
FashionMNIST 1	linear	90.47	91.63	86.78	89.63
	geodesic	<b>91.44</b>	<b>92.55</b>	<b>87.46</b>	<b>90.48</b>
FashionMNIST 2	linear	92.20	91.26	93.30	92.25
	geodesic	<b>93.56</b>	<b>91.80</b>	<b>94.12</b>	<b>93.16</b>
FashionMNIST 3	linear	72.46	79.58	83.16	78.40
	geodesic	<b>74.89</b>	<b>81.88</b>	<b>84.83</b>	<b>80.53</b>

Table: F1-Scores.



# Tweaking the Approximate Posterior

- The ELBO can be written as

$$ELBO = \log p_{\theta}(x) - \underbrace{\text{KL}(q_{\phi}(z|x) || p_{\theta}(z|x))}_{\approx 0 \text{ if } q_{\phi}(z|x) \approx p_{\theta}(z|x)}.$$

- Since the Kullback-Leiber divergence is always non-negative, the objective is to try to make it vanish by tweaking the approximate posterior  $q_{\phi}(z|x)$
- The idea is to add some Markov Chain Monte Carlo steps targeting the true posterior  $p_{\theta}(z|x)$  [SKW15]
- How to ensure that the model would still be amenable to the back-propagation ?

# Normalizing Flows

- The idea is to use smooth invertible parametrized mappings  $f_\psi$  to “sample”  $z$  [RM15]
- $K$  transformations are then applied to a latent variable  $z_0$  drawn from an initial distribution  $q$  (here  $q = q_\phi$ ) leading to a final random variable  $z_K = f_x^K \circ \dots \circ f_x^1(z_0)$  whose density writes

$$q_\phi(z_K|x) = q_\phi(z_0|x) \prod_{k=1}^K |\det J_{f_x^k}|^{-1}, \quad (1)$$

# Riemannian Hamiltonian VAE

- The idea relies on the **Riemannian** Hamiltonian Monte Carlo Sampler [GC11]
- We define a target density  $\pi$ :

$$p_{\theta}(x|z) = \frac{p_{\theta}(x, z)}{p_{\theta}(x)} \propto p_{\theta}(x, z) = \pi_x(z).$$

- An auxiliary **position-specific** random variable  $\rho \sim \mathcal{N}(0, \mathbf{G}(z))$  is introduced, the “momentum”
- The Hamiltonian writes





$$H_x^{Riem}(z, \rho) = U_x(z) + \frac{1}{2} \log((2\pi)^D \det \mathbf{G}(z)) + \frac{1}{2} \rho^{\top} \mathbf{G}(z)^{-1} \rho.$$

⇒ Make use of the “Generalized” Leapfrog integrator

Pros:

- The sampling is guided by the gradient of the true posterior





# References I

-  Christoph Baur, Shadi Albarqouni, and Nassir Navab, *Generating highly realistic images of skin lesions with GANs*, OR 2.0 Context-Aware Operating Theaters, Computer Assisted Robotic Endoscopy, Clinical Image-Based Procedures, and Skin Image Analysis, Springer, 2018, pp. 260–267.
-  Lei Bi, Jinman Kim, Ashnil Kumar, Dagan Feng, and Michael Fulham, *Synthesis of Positron Emission Tomography (PET) Images via Multi-channel Generative Adversarial Networks (GANs)*, Molecular Imaging, Reconstruction and Analysis of Moving Body Organs, and Stroke Imaging and Treatment, LNCS, Springer, 2017, pp. 43–51.
-  Clément Chadebec, Clément Mantoux, and Stéphanie Allasonnière, *Geometry-aware hamiltonian variational auto-encoder*, arXiv:2010.11518 [cs, math, stat] (2020).
-  Francesco Calimeri, Aldo Marzullo, Claudio Stamile, and Giorgio Terracina, *Biomedical data augmentation using generative adversarial neural networks*, International conference on artificial neural networks, Springer, 2017, pp. 626–634.

## References II


-  Clément Chadebec, Elina Thibeau-Sutre, Ninon Burgos, and Stéphanie Allasonnière, *Data augmentation in high dimensional low sample size setting using a geometry-based variational autoencoder*, arXiv preprint arXiv:2105.00026 (2021).
-  Maayan Frid-Adar, Idit Diamant, Eyal Klang, Michal Amitai, Jacob Goldberger, and Hayit Greenspan, *GAN-based synthetic medical image augmentation for increased CNN performance in liver lesion classification*, *Neurocomputing* **321** (2018), 321–331.
-  Mark Girolami and Ben Calderhead, *Riemann manifold langevin and hamiltonian monte carlo methods*, *Journal of the Royal Statistical Society: Series B (Statistical Methodology)* **73** (2011), no. 2, 123–214.
-  Mark Girolami, Ben Calderhead, and Siu A Chin, *Riemannian manifold hamiltonian monte carlo*, arXiv preprint arXiv:0907.1100 (2009).

## References III

-  Dimitrios Korkinof, Tobias Rijken, Michael O'Neill, Joseph Yearsley, Hugh Harvey, and Ben Glocker, *High-resolution mammogram synthesis using progressive generative adversarial networks*, arXiv preprint arXiv:1807.03401 (2018).
-  Diederik P. Kingma and Max Welling, *Auto-encoding variational bayes*, arXiv:1312.6114 [cs, stat] (2014).
-  Maxime Louis, *Computational and statistical methods for trajectory analysis in a Riemannian geometry setting*, PhD Thesis, Sorbonnes universités, 2019.
-  Yufei Liu, Yuan Zhou, Xin Liu, Fang Dong, Chang Wang, and Zihong Wang, *Wasserstein gan-based small-sample augmentation for new-generation artificial intelligence: a case study of cancer-staging data in biology*, *Engineering* **5** (2019), no. 1, 156–163.





## References IV

-  Ali Madani, Mehdi Moradi, Alexandros Karargyris, and Tanveer Syeda-Mahmood, *Chest x-ray generation and data augmentation for cardiovascular abnormality classification*, Medical Imaging 2018: Image Processing, vol. 10574, International Society for Optics and Photonics, 2018, p. 105741M.
-  Danilo Rezende and Shakir Mohamed, *Variational inference with normalizing flows*, International Conference on Machine Learning, PMLR, 2015, pp. 1530–1538.
-  Danilo Jimenez Rezende, Shakir Mohamed, and Daan Wierstra, *Stochastic backpropagation and approximate inference in deep generative models*, International conference on machine learning, PMLR, 2014, pp. 1278–1286.
-  Tim Salimans, Diederik Kingma, and Max Welling, *Markov chain monte carlo and variational inference: Bridging the gap*, International Conference on Machine Learning, 2015, pp. 1218–1226.

-  Hoo-Chang Shin, Neil A Tenenholtz, Jameson K Rogers, Christopher G Schwarz, Matthew L Senjem, Jeffrey L Gunter, Katherine P Andriole, and Mark Michalski, *Medical image synthesis for data augmentation and anonymization using generative adversarial networks*, International Workshop on Simulation and Synthesis in Medical Imaging, LNCS, Springer, 2018, pp. 1–11.
-  Hojjat Salehinejad, Shahrokh Valaee, Tim Dowdell, Errol Colak, and Joseph Barfett, *Generalization of deep neural networks for chest pathology classification in x-rays using generative adversarial networks*, 2018 IEEE International Conference on Acoustics, Speech and Signal Processing (ICASSP), IEEE, 2018, pp. 990–994.
-  Veit Sandfort, Ke Yan, Perry J. Pickhardt, and Ronald M. Summers, *Data augmentation using generative adversarial networks (CycleGAN) to improve generalizability in CT segmentation tasks*, Scientific reports **9** (2019), no. 1, 16884.



# References VI

-  Abdul Waheed, Muskan Goyal, Deepak Gupta, Ashish Khanna, Fadi Al-Turjman, and Plácido Rogerio Pinheiro, *Covidgan: data augmentation using auxiliary classifier gan for improved covid-19 detection*, *IEEE Access* **8** (2020), 91916–91923.
-  Junhao Wen, Elina Thibeau-Sutre, Mauricio Diaz-Melo, Jorge Samper-González, Alexandre Routier, Simona Bottani, Didier Dormont, Stanley Durrleman, Ninon Burgos, and Olivier Colliot, *Convolutional neural networks for classification of Alzheimer's disease: Overview and reproducible evaluation*, *Medical Image Analysis* **63** (2020), 101694.
-  Eric Wu, Kevin Wu, David Cox, and William Lotter, *Conditional infilling gans for data augmentation in mammogram classification*, *Image analysis for moving organ, breast, and thoracic images*, Springer, 2018, pp. 98–106.
-  Xin Yi, Ekta Walia, and Paul Babyn, *Generative adversarial network in medical imaging: A review*, *Medical image analysis* **58** (2019), 101552.